SpineLab: tool for three-dimensional reconstruction of neuronal cell morphology

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Abstract. SpineLab is a software tool developed for reconstructing neuronal feature skeletons from three-dimensional single- or multi-photon image stacks. These images often suffer from limited resolution and a low signal-to-noise ratio, making the extraction of morphometric information difficult. To overcome this limitation, we have developed a software tool that offers the possibility to create feature skeletons in various modes—automatically as well as with manual interaction. We have named this novel tool SpineLab. In a first step, an investigator adjusts a set of parameters for automatic analysis in an interactive manner, i.e., with online visual feedback, followed by a second step, in which the neuronal feature skeleton can be modified by hand. We validate the ability of SpineLab to reconstruct the entire dendritic tree of identified GFP-expressing neurons and evaluate the accuracy of dendritic spine detection. We report that SpineLab is capable of significantly facilitating the reconstruction of dendrites and spines. Moreover, the automatic approach appears sufficient to detect spine density changes in time-lapse imaging experiments. Taken together, we conclude that SpineLab is an ideal software tool for partially automatic reconstruction of neural cell morphology.

Keywords: SpineLab-software; graphical user interface; morphology reconstruction; neuronal feature skeleton; neurons; dendritic tree; spines; spine density changes.

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1 Introduction

Ever since the first descriptions of identified neurons by Camillo Golgi, 1 Santagio Ramon y Cajal, 2 and other pioneers in the field of modern neuroscience, morphometric data of identified neurons have contributed to our understanding of the nervous system. In recent years, morphometric analysis has gained in importance due to a series of exciting developments in the field of light microscopy, 3–4 the generation of genetically engineered mice expressing fluorescent proteins, 7 and modern computational approaches, which bring together complex morphological and functional data. 8–10 Accordingly, neuroscientists are confronted with the need to analyze neuronal structures and to extract morphometric information from huge datasets of single- or multi-photon image stacks.

Image stacks acquired with the help of laser-scanning microscopes often suffer from limited resolution and sometimes low signal-to-noise ratio, in part due to physical limitations. Therefore, we aimed at developing a software that supports the investigator in analyzing these datasets by providing automatic and manual tools integrated in a graphical user interface (GUI). This attempt resulted in a lightweight and easy to use software, operating even on average portable computers, which significantly accelerates morphometric analysis. We named this novel tool SpineLab. SpineLab is based on the NeuRA filter. 11–13

In the present study we validate the ability of SpineLab to reconstruct the dendritic tree of identified GFP-expressing neurons as well as its capability in identifying individual dendritic spines. Interestingly, a rather simple approach for automatic processing, not requiring computer processors with high power, proved to be sufficient to accelerate cell morphology reconstruction. Moreover, we demonstrate that this automatic approach is capable of detecting changes in spine density, when time-lapse imaging datasets are analyzed. Accordingly, SpineLab proves to be a valid and highly suitable software tool that significantly accelerates the morphometric analysis and three-dimensional (3-D) rendering of identified neurons.

2 Materials and Methods

2.1 Acquisition of Confocal Image Stacks

The datasets used in the present study were in part published previously in a different context. 14 Images were acquired with an upright Zeiss LSM Pascal confocal microscope. Dendritic trees were visualized using a 40x water immersion objective lens (0.9NA, Zeiss). A 63x water immersion objective lens (0.95NA; Zeiss) at 4x scan zoom was used to image individual dendritic segments at high resolution. Up to 40 images were recorded per stack (XY: 512 × 512 pixel, 0.11 μm/pixel and 0.07 μm/pixel; z-steps: 3 μm and 0.5 μm respectively; Videos 1 and 2).

2.2 Manual Quantifications

To verify the capability and correctness of the SpineLab tool to reconstruct neuronal dendritic branching and spines, four model cells were generated using NeuGen, 15 transferred to a volume...
image using NeuRA2,16 and reconstructed with SpineLab, Neurolucida software 10.0,17 and Neuronstudio 0.9.92 (CNIC Mount Sinai School of Medicine, NY18) (Fig. 1). In addition, a dendritic segment containing spines was generated using the above-mentioned method. These datasets were analyzed by independent investigators (Gerlinde Schuldt and Nadine Zahn).

The dendritic tree of individual GFP-expressing dentate granule cells9,20 was manually reconstructed using Neurolucida and Neuronstudio. Confocal image stacks of individual dendrites at higher magnification containing dendritic spines were assessed manually on 3-D image stacks of dendritic segments using the Zeiss LSM image browser to navigate through the stacks, as previously described.14,21,22 All dendritic protrusions were counted as dendritic spines, regardless of their morphology. Images from control and denervated dentate granule cells14,22 were analyzed blind to experimental condition to ensure unbiased observation. For each segment, a defined distance (σ=30 μm) from a dendritic branch point was analyzed and all spines were counted (red dots in Video 2). The spine density per μm was calculated based on these results. All results were compared with partially automatic reconstructions by the same independent investigators using SpineLab.

2.3 SpineLab Software Tool

SpineLab is based on the morphology reconstruction software NeuRA2,16 which is an optimized and extended version of the award-winning Neuron Reconstruction Algorithm NeuRA.11–13 SpineLab was developed for an automatic or partially automatic extraction of 3-D data, such as morphometric data of neurons, from image stacks suffering from reduced z-resolution. SpineLab combines simple noise reducing and segmentation operators, like median-filtering or global segmentation,23 as well as the inertia based anisotropic diffusion filter, introduced in Refs. 11–13, together with the possibility to extract centerlines, using Telea’s Augmented Fast Marching Method.24

SpineLab enables the user to modify the reconstruction manually via a highly developed graphical user interface. It was written in C++, using the Qt-GUI-Framework,25 and is therefore available for Mac, Linux, and Windows systems. All methods integrated in SpineLab are implemented highly optimized, yielding a software tool, which requires few resources and runs reliably and fast on today’s computers.

2.4 Pre-Processing of Three-Dimensional Image Stacks

In a first pre-processing step, SpineLab applies a median filter23 with a small neighborhood size to all original images in order to reduce noise. Thereafter, the image stacks are projected along the z-axis using the maximum norm

\[ u_z(x, y) = \max_{\zeta} u(x, y, \zeta), \]

where \( u \) denotes the image stack, depending on the 3-D coordinates \((x, y, z)\) and \( u_z \) denotes the projected image, depending on the two-dimensional (2-D) coordinates \((x, y)\).

2.5 Generation of Neuronal Feature Skeletons

The projected image stacks [Fig. 2(a)] are segmented [Fig. 2(b), for details see Ref. 23] and the centerlines of the segmented regions are extracted using Telea’s Augmented Fast Marching Method24 [Fig. 2(c)], which collapses the boundaries of the segmented image parts. The centerlines are subsequently transformed into the so called neuronal feature skeleton—a graph26 consisting of nodes and edges linking the nodes [Fig. 2(d)]. To obtain the feature skeleton from the centerline, every pixel belonging to the centerline is considered to be a skeleton node. The nodes belonging to adjacent pixels are linked with edges. Nodes with one or three neighbors represent end points of spines and dendrites or branching points, respectively. Nodes with exactly two neighbors are important to approximate the curvature of dendrites or spines. However, a subset of these nodes can be removed if the angle between the two adjacent edges is large (i.e., >135 deg). This simplification yields a neuronal feature skeleton, which consists of a reasonable number of nodes [Fig. 2(e)]. This feature skeleton is 2-D, since the original image stack was projected along the z-axis. In a final step, the z-coordinate

\[ s_z = \frac{\sum z \cdot u(x, y, z)}{\sum u(x, y, z)} \]

of every skeleton node is therefore calculated as the center of mass along the z-axis of the pre-processed image stack \( u(x, y, z) \). This yields a 3-D skeletal representation of neurons or dendrites with spines of interest—the so called neuronal feature skeleton.

2.6 Analyzing the Neuronal Feature Skeleton

The neuronal feature skeleton can be used to extract additional information from imaging datasets—in particular spine length and spine volume. To obtain this information, the feature skeleton \( G \) is defined as a special graph with following attributes: (1) \( G \) is connected and contains no cycles (i.e., \( G \) is a tree26); (2) \( G \) is weighted,26 and the weights symbolize the real length in micrometers (i.e., every edge of the graph is attributed with its real length); (3) one path of \( G \) (usually the longest path in the graph) represents the dendrite; (4) branches connected to the...
dendrite represent single spines. Spines in z-direction were not included in this analysis.

The volume of single spines can only be calculated if they are oriented in the x- and y-axes. Spines are cut away from the dendrite on the image level and reconstructed via the Neuron Reconstruction Algorithm NeuRA\textsuperscript{11-13} in the version NeuRA\textsuperscript{2,16} where the originally used Marching-Tetrahedron mesh generator\textsuperscript{27} was replaced by the faster Marching-Cubes-Algorithm.\textsuperscript{28} The volume of these spines can easily be calculated by using Gauss’ divergence theorem.\textsuperscript{29}

3 Results

In the present study, model neurons generated with NeuGen,\textsuperscript{15} as well as the dendritic arbor of cultured dentate granule cells of entorhino-hippocampal slice cultures prepared from Thy1-GFP mice,\textsuperscript{7} were reconstructed (Figs.1–3). In addition individual dendritic segments were evaluated at high magnification (Figs. 4–6) to test and validate handling and accuracy of the newly developed reconstruction software SpineLab.

3.1 SpineLab

One of the central problems in cell morphology reconstruction using transgenic mouse lines, which express fluorescent markers for visualization of neuronal morphology, is the fact that single- or multi-photon image stacks usually contain several cells, one of which should be reconstructed (Figs. 1–3). In addition individual dendritic segments were evaluated at high magnification (Figs. 4–6) to test and validate handling and accuracy of the newly developed reconstruction software SpineLab.

Fig. 2 Reconstruction of GFP-labeled neurons using SpineLab: (a) through (d) Projected image stacks of a GFP-expressing dentate granule cell; (b) Segmentation using a threshold method in SpineLab’s graphical user interface; (c) Using Telea’s Augmented Fast Marching Method the centerlines of the segmented region are generated; (d) The centerlines of the regions of interest are selected by rolling over with the mouse. Scale bars: 10 μm; (e) To ease separation and to confirm correct reconstruction of individual neurons, SpineLab offers a real-time z-plane view, in which the investigator can correct the precise position of the centerline in all spatial directions. The blue squares denote the skeleton nodes whereas the green lines denote the skeleton edges. The eight labeled nodes are arbitrarily chosen to highlight the z-plane view. Scale bars 2 μm; (f) The dendrogram of the reconstructed neuron. Different colors indicate different branch orders; (g) Examples of values computed by SpineLab. The particular branches and angles are shown in Fig. 2 (f). (Video 1 QuickTime, 2.8 MB) [URL: http://dx.doi.org/10.1117/1.JBO.17.7.076007.1].
Values in differences were within re-test reliability [SpineLab (1) versus SpineLab (2)]. Values in \( \mu m \), SEM, standard error of the mean.

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<td>1078 \pm 51</td>
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Fig. 3 Validation of SpineLab reconstruction of GFP-labeled neurons with Neurolucida and Neurostudio: Five individual GFP-expressing dentate granule cells of entorhino-hippocampal slice cultures\(^{14}\) were reconstructed using SpineLab, Neurolucida, and Neurostudio software to validate the newly developed software tool. The results revealed comparable total dendritic branch length values. No significant differences were detected between the three software tools. The observed differences were within re-test reliability [SpineLab (1) versus SpineLab (2)]. Values in \( \mu m \), SEM, standard error of the mean.

3.2 Reconstruction of Dendritic Trees Using SpineLab

We have used SpineLab to reconstruct the morphology of the dendritic trees of individual cultured GFP-expressing neurons (Fig. 2). After applying a median filter\(^{23}\), the image stacks were projected along the \( z \)-axis using the maximum norm [Fig. 2(a); see Sec. 2] and segmented using a threshold method, which is reasonable, since the data resolution in \( z \)-direction is low compared with the horizontal resolution; every pixel of the projected image with a higher intensity than the selected threshold is colored orange and every pixel with a lower intensity than the selected threshold is colored black\(^{23}\), as shown in Fig. 2(b). The centerline of the segmented region [Fig. 2(c)] was then extracted by using Telea’s Augmented Fast Marching Method\(^{24}\), which generates centerlines from segmented 2-D images by collapsing the boundaries of the segmented parts. Parts, which belong to the cell of interest, can be selected by the investigator by defining regions of interest with the computer mouse [Fig. 2(d)]. In addition, SpineLab provides a real-time \( z \)-plane view supporting separation and precise position of centerlines, and therefore the identification and separation of individual dendritic branches belonging to different neurons [Fig. 2(e)]. The resulting 3-D neuronal feature skeleton is a tree in the sense of graph theory, which means it is a connected graph without cycles\(^{26}\), for which the root denotes the soma. This enables the visualization of the reconstructed dendritic tree as a dendrogram [Fig. 2(f)] and subsequent assessment of various morphometric parameters of interest. Starting at the soma, the lengths and orders of the dendritic branches and the angles between branches emerging from identified branching points can be automatically computed [Fig. 2(g)]. Using this approach, a trained investigator can reconstruct individual cultured dentate granule cells within \( \approx 10 \) min, i.e., an approximate total dendritic length of 1000 \( \mu m \).

3.3 Validation of Dendrite Reconstruction Using SpineLab

We validated the reliability and accuracy of SpineLab in dendritic reconstruction in two steps: First, model neurons with known dimensions were generated using NeuGen\(^{15}\) [Fig. 1(a)] and reconstructed with SpineLab [Fig. 1(b)], Neurolucida\(^{17}\) and Neurostudio\(^{18}\) software. Second, we compared the results of SpineLab reconstructions of GFP-expressing neurons with the results of Neurolucida and Neurostudio. We observed differences of \( \leq 1.5\% \) while reconstructing model cells [Fig. 1(c)] and differences of \( \leq 6\% \) between the reconstructions of GFP-labeled neurons done with SpineLab compared to Neurostudio and Neurolucida software (Fig. 3). Taken together, we conclude that SpineLab is a reliable tool to determine dendritic branch lengths in 3-D image stacks, especially since SpineLab yielded accurate results in reconstructing the model neurons (which was also the case for Neurolucida and Neurostudio-software).

3.4 Reconstruction of Identified Dendritic Segments and Dendritic Spines

Next we assessed the ability of SpineLab to reconstruct and trace dendritic spines. In particular, we were interested in evaluating how many of the present dendritic spines could be automatically identified (Fig. 4). To obtain the neuronal feature skeleton from the projected image [Fig. 4(a)], the same approach was used as in the case of reconstructions of the entire dendritic tree of neurons: A centerline of the projected image was generated using NeuGen\(^{15}\), i.e., an approximate total dendritic length of 1000 \( \mu m \).

15 MB of hard disk space and low memory resources required) and easy to handle software for partially automatic cell reconstructions, which supports investigators with a set of automatic tools to identify and reconstruct neuronal morphology. All necessary parameters for noise reduction, segmentation, and centerline-extraction can be adjusted in real-time by the operator.
calculated and transformed to the neuronal feature skeleton, as described (see Sec. 2). The longest path of the resulting feature skeleton is marked as dendrite, which is correct for most images and can be changed by the operator if necessary [Fig. 4(c)]. The endpoints of the spines are detected reliably by the automatic approach of SpineLab, whereas the startpoints of the spines have to be corrected manually in most cases. The reconstruction of each dendritic segment can be saved as a spinogram [Fig. 4(d)].

### 3.5 Spine Density Analysis Using SpineLab

Since dendritic spines, especially the neck of spines, are close to and in part beyond the resolution of confocal microscopy, the reconstruction algorithm described above did not detect all spines. To improve the automatic analysis, disconnected skeleton parts, which are often spine heads, were automatically connected to the dendrite by adding the shortest edge, which connects the dendrite and the spine head. Nevertheless, due to low resolution in z-direction, spines oriented in the z-axis, were detected only occasionally. We believe that this reflects the rather low detection rate of $31 \pm 2.1\%$ ($n = 10$ segments) using the initial automatic approach in comparison to manual assessment of all spines in three-dimensions [Fig. 5(a); Video 2]. Regardless of these limitations, SpineLab significantly accelerated the analysis of spine densities since a considerable portion of spines were detected by the automatic approach of the software.

### 3.6 Spine Density Changes Using SpineLab

It has been suggested in a consensus paper by several labs that only spines exceeding the dendrite laterally should be analyzed in order to minimize errors, due to the low z-resolution of the image stacks.$^{30}$ In fact, the reliability of SpineLab to detect the subset of lateral spines in dentate granule cells was considerably higher (>80%; Fig. 4(c)), in comparison to detecting spines in all three dimensions (Fig. 5). In order to base the analysis of lateral spines on objective criteria, a function was included, which enables setting a lateral angle in which all spines will be considered. Using this specification, we reasoned that the reliability of assessment of changes in spine density by SpineLab should be particularly high if the same dendritic segment is visualized repeatedly. Thus SpineLab should be able to detect changes of spine density without the need of time-consuming and laborious post-hoc manual corrections. To test this hypothesis, dendritic segments of untreated controls and partially denervated dentate granule cells were analyzed.$^{14,22}$ In this earlier studies we were able to demonstrate that denervation leads to a reduction in spine densities of about 30% to 40% at seven days post lesion. Indeed, the automatic pre-processing approach of SpineLab reliably detected these changes in spine density $[-37 \pm 0.1\%; p = 0.55$ in comparison to manual assessment; Fig. 5(b)]. Accordingly, we were able to confirm our previous result on denervation-induced changes in spine density using an objective computer-based approach, i.e., the SpineLab software.

Taken together, we conclude that while automatic spine detection of SpineLab fails to identify all dendritic spines and requires manual correction, it identifies a considerable portion of all spines, in particular lateral spines,$^{30}$ and thus appears suitable for detecting relative changes in spine density. This makes SpineLab an attractive tool for screening huge time-lapse imaging datasets for spine density changes in a rather short period of time, specifically compared with manual assessments. In case a difference is detected, a manual post-hoc analysis could be performed to verify these results.

### 3.7 Spine Length and Spine Volume Analysis

One of the major advantages of SpineLab reconstruction is that the neuronal feature skeleton can be used to extract additional information from imaging datasets. In particular spine length and spine volume are considered important functional features of dendritic spines (for a recent review on spines and their function see Ref. 31). SpineLab automatically measures the length of spines and provides a function for volume calculation of selected spines. In Fig. 6(b) the surface reconstruction, on which the volume calculation is based on (for details see Sec. 2) is shown for some spines. Naturally, these extracted values are limited by the resolution of the confocal laser scanning microscope. However, their automated extraction again provides the opportunity to use this approach to assess relative changes in spine length and spine volume of large numbers of spines under

![Fig. 6 3-D surface rendering of dendritic spines: (a) Individual spines can be processed by SpineLab using three-dimensional surface rendering. Projected image of the dendritic segment shown in Fig. 4. Scale bar 2 µm. (b) The spine indicated in (a) by an arrow is shown after 3-D surface rendering from two sides. (c) Additional examples of spines indicated in (a) by numbers. SpineLab can extract information about the length and volume of spines.

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Fig. 5 SpineLab detects changes in spine density: (a) and (b) The spine density of ten dendritic segments (five segments imaged twice, at 0d and 7d) was assessed manually and compared to the automatic detection-step of the SpineLab-software. While SpineLab was only capable of detecting $31 \pm 2.1\%$ of spines in comparison to a manual analysis in three dimensions it showed robust results when changes in spine density were compared to values of manual reconstruction. (Video 2 QuickTime, 1.9 MB) [URL: http://dx.doi.org/10.1117/1.JBO.17.7.076007.2].
various experimental conditions, as long as the same dendritic segment is imaged with the same parameters at the same microscope.

### 3.8 Validation of Spine Reconstruction

To provide further evidence for the accuracy of SpineLab to detect dendritic spines, we generated and reconstructed a model dendritic segment studded with 57 equally distributed spines. The automatic approach detected the dendrite (error $\approx 1.2\%$) and $45(\approx 80\%)$ of the spines correctly. As expected, spines oriented in z-direction were not detected. After manual correction, all spines were reconstructed correctly with an average error of $\approx 0.3\%$ per spine. These results show that SpineLab is a suitable tool to accelerate detection and analysis of dendritic spines.

### 4 Discussion

In the present study we have introduced a novel partially automatic software tool, named SpineLab. We report that: (1) SpineLab is a lightweight and easy to use program that enables investigators to adjust all necessary parameters of image pre-processing and automated detection in real-time. (2) SpineLab facilitates the reconstruction of neurons by combining automatic and manual approaches. (3) We validate the ability of SpineLab to facilitate assessment of dendritic arbors of identified fluorescent neurons in confocal image stacks. (4) Furthermore, we demonstrate that SpineLab is capable of detecting dendritic spines, in particular lateral spines, and determining changes in spine density in time-lapse imaging datasets. Taken together, we conclude that SpineLab complements the available software tools of neural morphology reconstruction and will therefore be of value for the neuroscience community.

The importance of valid, reliable, and fast reconstruction and assessment of neural morphology is reflected in the fact that a series of tools is available on the market in both commercial as well as freeware versions. Such tools sometimes claim a fully automated detection or reconstruction of morphology information at high accuracy. If the best images available are used to assess the capability of such software, this may indeed be true. However, typical experimental data does not consist of ideal images (e.g., such as in the case of the model cells used in the present study), which resides in part also in physical limitations of the imaging techniques (e.g., visualization of structures below the diffraction limit such as the neck of dendritic spines). We therefore developed a lightweight and easy to use software tool with low hardware requirements (even running on average portable computers), which supports investigators in assessing neural morphology by pre-processing and automatically detecting at least parts of the structures of interest.

An important aspect of this approach is the real-time adjustment of parameters for automated detection. This feedback mechanism ensures low failure rates since the investigator gets a visual feedback while adjusting the parameters to get ideal results in the first step of automatic reconstruction. The value of such an approach has been recognized by many other groups and companies and has been implemented in the latest versions of their reconstruction tools (e.g., latest version of IMARIS 3D, Bitplane).

Novel software tools need to be validated. We have, therefore, analyzed the ability of SpineLab to reconstruct the entire dendritic tree of model neurons and have compared SpineLab reconstructions of identified GFP-expressing granule cells with reconstruction results of the same neurons obtained with Neurolucida and Neuronstudio software. The analysis revealed comparable results with the expected small deviations. Thus, SpineLab is a valid and reliable tool to reconstruct and assess the morphology of dendritic trees.

The automatic approach of SpineLab was able to detect $\approx 30\%$ of all dendritic spines on a given dendritic segment imaged at high resolution in our time-lapse imaging datasets. This may reside, at least in part, in the fact that live cell imaging has to take phototoxic damage into account and thus signal-to-noise ratio and $z$-resolution will be lower in comparison with images taken from fixed tissue mounted in antifading medium and imaged with oil immersion objectives. This will inevitably lead to a lower detection rate of spines specifically in $z$-direction. In fact, it has been recognized that even under “ideal imaging conditions” the limited resolution in $z$-dimension can be problematic with respect to spine analysis. It has been therefore proposed in a consensus paper by several labs that only lateral spines, i.e., spines in $x$-$y$-direction, should be analyzed. Indeed the ability of SpineLab to detect these spines in our datasets was high ($>80\%$) and failed primarily in cases where optical fusion of neighboring spines occurred in the 2-D-projected images. In line with the high rate of detection of lateral spines, we were able to demonstrate that the automatic spine detection approach of SpineLab is capable of detecting relative changes in spine density in time-lapse imaging datasets. This is an important result as it will facilitate the analysis of large datasets for changes in spine density in a considerably short period of time. Given the fact that organotypic slice cultures are a highly versatile and widely used in vitro model, we are confident that the usage of single- or multi-photon imaging techniques in combination with SpineLab will significantly accelerate assessment of spine density changes under various experimental conditions of interest. This may in particular be interesting for high-throughput approaches such as screening for drugs that could be aimed at affecting spine densities in neuronal networks.

It may be important to mention that the SpineLab reconstructions can be exported to the .svc-file format. This is in particular of value, since SpineLab is primarily focused on extracting the neuronal feature skeletons but not in further detailed analysis of the respective spine- or dendrograms. Thus feature skeletons obtained with SpineLab can easily be transferred to other software tools for further analysis and computational modeling, e.g., to the TREES Toolbox or the simulation environment NEURON.

Finally, SpineLab is capable of rendering individual spines in three dimensions. This feature of SpineLab enables investigators to assess relative changes in the volume of spines, as long as the same parameters are used when imaging identified dendritic spines repeatedly. However, due to technical reasons residing in the imaging approach itself, this is currently only possible for spines oriented in $x$- and $y$-directions. Conventional single- and multi-photon microscopes do not yield correct absolute volumetric data. The recent development of novel microscopic techniques offers the opportunity to overcome this limitation, since absolute measurements of small (0.1 to 0.5 μm) microscopic structures seem to be within reach. It can be expected that SpineLab will yield useful absolute volumetric data if imaging datasets from these microscopes are used.

We conclude that SpineLab is a useful and easy to handle tool for the extraction of morphometric data from single- or multi-dimensional imaging datasets.
multi-photon image stacks of neurons. We are confident that it will be of value for the neuroscience community, in particular by accelerating the analysis of spine density changes.

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