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Abstract. We demonstrate a record bandwidth high energy supercontinuum source suitable for multispectral photoacoustic microscopy. The source has more than 150 nJ/10 nm bandwidth over a spectral range of 500 to 1600 nm. This performance is achieved using a carefully designed fiber taper with large-core input for improved power handling and small-core output that provides the desired spectral range of the supercontinuum source.

Keywords: supercontinuum; light; energy; photoacoustic.

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1 Introduction

Photoacoustic microscopy (PAM) is an absorption-based and depth-resolved imaging technique that combines optical excitation of a zone of interest with ultrasonic detection of the created waves.¹ A high-pulse energy laser illuminates biological tissue, where molecules absorb the optical energy. A rapid thermoelastic expansion generates broadband, high-frequency ultrasonic (acoustic) waves that are used to reconstruct a depth-resolved map of the optical absorption region. A two-dimensional scanning of the excitation laser allows acquisition of a three-dimensional functional image. Absorption spectra of several main absorbers contained in human tissue are shown in Fig. 1.

For functional bioimaging based on absorption, the window of interest is between 200 and 2000 nm approximately. Using multiple wavelengths in so-called functional PAM allows both imaging and differentiation of multiple absorbers within a sample. A typical example is the imaging of melanomas, where wavelengths around 584 and 764 nm can be used to differentiate hemoglobin and melanin and thereby differentiate the melanoma from the surrounding vasculature.⁹

Originally, PAM was demonstrated using single-wavelength lasers as the optical excitation source, such as an Nd:YAG Q-switched laser at 1064 nm or frequency-doubled to 532 nm, or dye lasers. The pulse width is typically 1 to 10 ns with a pulse repetition rate in the hertz to tens of kilohertz range.¹⁰⁻¹² Fixed single-wavelength sources made such systems heavily reliant on sample absorption at or near the laser wavelength and are not suitable for multispectral PAM. Optical parametric oscillators (OPOs) have been used for multispectral functional PAM to allow wavelength tunability, reaching a broad tuning range covering 270 to 1300 nm.¹³ However, OPOs have a low pulse repetition rate and are bulky and expensive. Stimulated Raman scattering fiber-laser sources have also been used for multispectral functional PAM; however, the accessible wavelengths were limited.¹⁴

These limitations can be circumvented using a broadband supercontinuum source, which today can be constructed to have over two octaves of bandwidth from about 500 to above 2200 nm,¹⁵ and can be used in conjunction with optical bandpass filters, such as acousto-optic tunable filters to select the suitable emission wavelength that would allow a fast tunability between different wavelengths (typically tens of kilohertz). Such a strategy would allow multispectral functional PAM capable of interrogating samples containing a wide range of absorbers using a single optical source. However, even state-of-the-art supercontinuum sources do not deliver enough pulse energy to make them suitable for use in multispectral PAM, which requires more than 1.25 nJ/nm.¹⁶,¹⁷

Here, we address this issue and present a careful design of a nonlinear fiber for spectral broadening, which is fabricated by tower tapering and combines a large-core input fiber for high-pulse energy handling with a small-core fiber that gives the desired spectral bandwidth. With this nonlinear fiber, we achieve a supercontinuum source with a pulse energy density above 15 nJ/nm over a broad bandwidth of 500 to 1600 nm.

2 Fiber Taper Design

Our aim is to increase the pulse energy density of the supercontinuum source over a bandwidth as broad as possible, ideally covering at least the 500 to 1000 nm wavelength range. The pulse energy scales with the pulse width and the peak power. For PAM, the pulse width is typically 1 to 10 ns to enable stress and thermal confinement.¹⁸ Hence, to increase the pulse energy density in a certain wavelength band of the supercontinuum spectrum, a pump laser with a pulse width close to the maximum
10 ns should be used, and the pulse peak power in that band must be increased.

Supercontinuum sources typically comprise a pump laser coupled into a highly nonlinear fiber. To increase the peak power within a specific wavelength range one can (1) increase the pump peak power, which will both increase the power and change the spectral profile of the supercontinuum, or (2) change the fiber design to spectrally shape the supercontinuum and move power from a nonimportant wavelength range into the desired wavelength range. We report on a method using both solutions.

Most common commercial supercontinuum sources use a microstructured photonic crystal fiber (PCF) with a small-core diameter, both to move the zero-dispersion wavelength (ZDW) below the pump laser wavelength of 1064 nm and to achieve a certain blue edge, typically below 500 nm. Standard supercontinuum PCFs have a guiding core diameter of <5 μm surrounded by a microstructure consisting of air holes of diameter d with a relative hole diameter, or air-hole diameter to pitch ratio (d/Λ), of around 0.5 (e.g., the SC-5.0-1040 from NKT Photonics), and generate a broad spectrum with a blue edge around 475 nm and a red edge above 2300 nm.

The small core increases the effective nonlinearity of the fiber and thus the efficiency of the supercontinuum generation (SCG), but it also limits the power-handling capability. Since the maximum optical pulse peak power a fiber can handle is linked to the energy per surface area at a given pulse width, it would be desirable to use a larger core fiber to allow higher energy pulses to be coupled into the fiber. However, since the nonlinearity is inversely proportional to the effective mode area, simply increasing the core diameter leads to less efficient SCG, in particular if it moves the ZDW above the pump wavelength so that the pump is in the normal dispersion regime. More importantly, by increasing the core diameter, the blue edge of the spectrum is typically shifted to longer wavelengths, reducing coverage of the PAM window.

Our solution is to use a carefully designed PCF taper, which connects an input and output PCF, each with their carefully chosen designs: a large-core fiber that can handle high-pulse energy at the input and a standard highly nonlinear small-core PCF at the output that produces the desired blue edge of the output spectrum. Tapered fibers were used early on for SCG and have been thoroughly studied in terms of how they shift the dispersion wavelength and supercontinuum spectral edges (see Refs. 19 and 20 for recent reviews).

The simplest tower tapering method only changes the drawing speed in order to make the taper and thereby, to a good approximation, maintains the relative hole diameter d/Λ while reducing the hole-to-hole pitch A. In this case, there is an optimum pitch that gives the shortest blue edge determined by group-velocity matching to the red edge. For a relative hole diameter of 0.52, the optimum pitch is, for instance, 2.6 μm, which results in a blue edge of around 479 nm depending on the infrared loss edge. Interestingly, this optimum pitch is typically the one for which the second ZDW crosses the infrared loss edge of the fiber. The amount of power in the blue edge is determined by so-called group-acceleration matching and decreases with the steepness of the taper (i.e., long tapers have more power closer to the blue spectral edge).

While most of the focus in fiber tapering has been on expanding spectral coverage at the blue edge, it should be mentioned that theoretical work has also been done on designing special taper profiles that allow to manipulate the red edge in terms of optimizing the Raman-induced soliton self-frequency shift.

When tapering PCFs in particular, a more complicated strategy of draw tower tapering is employed, where both the draw speed and the pressure on the air holes are controlled. Such a strategy allows optimum control of the air hole microstructure along the taper. This was used to make a supercontinuum PCF taper with a single-mode input (d/Λ = 0.52, A = 3.3 μm) and a large relative hole diameter at the output (d/Λ = 0.85, A = 2.2 μm) for obtaining a deep-blue supercontinuum with a blue edge at 375 nm.

In view of these results and general design rules, we choose here simple tower tapering where only the drawing speed is varied to change the core diameter with a fixed relative hole diameter. This gives the best taper reproducibility and is sufficient here since we have chosen two input and output PCF designs.

**Fig. 1** Absorption coefficients of several main absorbers contained in human tissue. The graphs for water have been drawn by adapting data from Refs. 2–4. The graph for the melanin (melanosomes) was inferred using Eq. (8) in Ref. 5. Oxygenated and deoxygenated blood graphs have been obtained by adapting data from Refs. 6 and 7. The graph for human fat has been drawn using data from Ref. 8. 260 and 280 nm are the relevant wavelengths used for DNA, RNA base identification, and DNA/proteins ratio measurement.
that have the same relative hole diameter of 0.52. To avoid too much spectral broadening in the tapered section connecting our two fiber sections, we use rather short 0.5 to 1 m tapered sections. The fiber output section is similar to a standard supercontinuum fiber with a 5 μm core diameter and the input section is a larger core fiber with a core diameter above 10 μm for increased power handling. The ZDW of the input section of the fiber is above 1170 nm, and thus we are pumping 100 nm into the normal dispersion regime of a large-core fiber with long pulses. Significant spectral broadening is therefore not expected before the optical pulse reaches near the end of the tapered section where the ZDW crosses the pump wavelength of 1064 nm.

3 Experimental Setup and Specific Fibers

The experimental setup is shown in Fig. 2. A 1064-nm Elforlight laser (Model FQS-400-1-Y-1064) emitting pulses with a duration of 4 ns, a repetition rate of 1 kHz, and pulse energies of up to 500 μJ is used as pump laser. A half-wave plate (HWP) and a polarizing beam splitter (PBS) allow for continuous adjustment of the laser power, while an aspheric lens (AL) is used to couple the pump into the PCF. The AL focal length is optimized for each PCF in order to maximize the coupling efficiency. The PCF input end is fixed to a NanoMax three-axis precision translation stage, and the angle of the input beam with respect to the AL can be adjusted with two steering mirrors in order to optimize coupling, which for this work was typically around 60%, so that the total output energy of the supercontinuum is typically around 20% to 30% of the pump laser. An integrating sphere is used to collect the output signal and relay it to an optical spectrum analyzer (OSA) via a large-core step-index fiber. Two separate OSAs are used in order to record the full spectrum, one with a scanning range from 350 to 1750 nm (Yokogama, Ando AQ6315) and a second one covering a range from 1200 to 2400 nm (Yokogama, AQ6375). A broadband power meter (Ophir Photonics, 3A-QUAD) is used to measure the total optical power in the supercontinuum. The supercontinuum spectrum is then calibrated using all measurements and plotted in terms of energy density in nJ/nm.

We tested five different PCFs drawn by NKT Photonics, four of which were specially designed for this study with an approximately fixed relative hole diameter of 0.52. There are three straight PCFs with core diameters of 5 (SC-5.0-1040), 9 (PCF-9), and 10 μm (PCF-10) and two PCF tapers with an input core diameter of ~10 μm tapered down to 5 μm over a length of 0.5 to 1 m (tapers 10.3-5 and 10.7-5). The specific longitudinal profile and the input and output end facets of the tapered fibers are given in Fig. 3.

4 Experimental Results

For each of the five PCFs, we measure the pump pulse energy it can transmit before damage occurs and the supercontinuum spectrum at a pump pulse energy just below the damage threshold. Figure 4 shows the damage threshold for several PCF input core diameters and illustrates the linear dependence of the damage threshold with the core area at the input end of the fiber. More importantly, we see no difference between the straight fibers and tapered fibers with similar input core diameter. Hence, the damage threshold of the tapered fibers is that of the input fiber; that is, no damage occurs within the tapered and straight sections.

We conclude that the input core diameter is, as we thought, the relevant parameter for determining the maximum permissible energy that can be coupled into a PCF.

Figure 5 shows the supercontinuum spectrum generated by each of the standard PCFs (SC-5.0-1040, PCF-9, and PCF-10) and the taper designated as 10.7-5. The optical spectra have been recorded using an input energy corresponding to ~70% to 90% of the damage threshold.

Table 1 lists the core diameter, the total supercontinuum output pulse energy, the visible pulse energy, and the theoretical and experimental blue edges. The visible energy is measured by filtering out the light above 850 nm and the blue edge is evaluated at the 2 nJ/nm level.
The spectra shown in Fig. 5 confirm that the tapered fiber indeed provides a much higher pulse energy density while simultaneously emitting a supercontinuum with a blue edge that remains at 475 nm. We also see that the large-core straight fibers perform equally as well as the tapered fiber in terms of power handling; however, the blue edge is too far shifted toward longer wavelengths to be of any use for functional multispectral PAM. Table 1 shows that the available visible pulse energy from fibers performs equally as well as the tapered fiber in terms of bandwidth, covering 500 to 1600 nm. This source, when combined with optical bandpass filters, can serve functional multispectral PAM applications.

The supercontinuum output energy can be further scaled up by increasing the input core diameter and then use a pump source with a higher peak power. The pulse width cannot be increased much from the 4 ns values used here, due to the inherent restrictions in PAM, which requires stress and thermal confinement.

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### References


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Christian Jakobsen is a development engineer at NKT Photonics with main activities in developing optical fibers and fiber manufacturing processes. He has a PhD in optical physics and has been active in research and development within manufacturing of optical fibers for the past 20 years. He is inventor and co-inventor of a number of patents and author and coauthor of a number of papers in peer-reviewed journals.

Keith Oakes is a founding director of Elforlight Ltd. His role is focused on design and development of nanosecond DPSS lasers and OPOs. He graduated from Hull University in 1980 with BSc joint honors in physics and geology. He has spent 35 years working in laser research, development, and design.

PETER MORTEN MOSELUND has worked for nine years with pulsed fiber lasers and supercontinuum generation. For the last four years, he has worked mainly on mid-IR supercontinuum generation as the technical manager of NKT Photonics activities in this field. He authored or coauthored more than 35 refereed articles, nearly all within the field of supercontinuum generation and its applications (369 citations, h-index 12). In addition, he is the inventor or co-inventor of two patent families.

Lasse Leick is heading the external projects and IPR Group at NKT Photonics. He has a PhD in components for optical telecommunications, and since 2006 he has been working on ultrashort pulsed lasers and supercontinuum sources. He has authored or coauthored more than 30 refereed articles (371 citations, h-index 11). In 2012, he received the Danish National Advanced Technology Foundation’s Pasteur Prize, which is given to the project leader of the year.

Ole Bang is a professor at the Technical University of Denmark and Fellow of OSA. He heads the Fiber Sensors & Supercontinuum Group, who develops photonic crystal fibers for sensing and supercontinuum lasers and use them for applications in imaging and spectroscopy. He has published 180 journal papers with 6040 ISI citations and ISI h-index 44. He holds several patents within supercontinuum lasers and polymer optical fiber sensors and is co-founder of SHUTE Sensing Technologies.

Adrian Podoleanu is a professor of biomedical optics at the University of Kent, UK, and he is a fellow of OSA, SPIE, and IOP. He leads the research of the Applied Optics Group, oriented on high resolution noninvasive optical imaging. The awards he received are Royal Society Wolfson Research Merit Award 2015; ERC Advanced Research Fellowship, 2010 to 2015; Ambassador’s Diploma, Embassy of Romania in UK, 2008; Leverhulme Research Fellowship, 2004 to 2006; and the Romanian Academy Constantin Miculescu Prize, 1984.