Impact of hemoglobin breakdown products in the spectral analysis of burn wounds using spatial frequency domain spectroscopy

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Abstract. Burn wounds and wound healing involve several biological processes that may complicate the interpretation of spectral imaging data. Through analysis of spatial frequency domain spectroscopy data (450 to 1000 nm) obtained from longitudinal investigations using a graded porcine burn wound healing model, we have identified features in the absorption spectrum that appear to suggest the presence of hemoglobin breakdown products, e.g., methemoglobin. Our results show that the calculated concentrations of methemoglobin directly correlate with burn severity, 24 h after the injury. In addition, tissue parameters such as oxygenation (\(\text{SiO}_2\)) and water fraction may be underestimated by 20% and 78%, respectively, if methemoglobin is not included in the spectral analysis.

Keywords: burns; hemoglobin; methemoglobin; spectroscopy; multispectral imaging; spatial frequency domain spectroscopy.

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There are several physiological parameters associated with burn wounds and wound healing that can be detected and quantified optically. Structural changes to tissue from thermal insult (collagen denaturation, protein coagulation, etc.) can be detected by changes in light scatter through tissue (i.e., reduced scattering coefficient). Similarly, changes in functional characteristics, such as tissue oxygen saturation, blood volume, and water fraction, (edema) can be monitored by how tissue absorbs light (i.e., absorption coefficient).1,2 In the case of thermal burn wounds and its subsequent wound healing response, however, there are biological processes (e.g., extravasation, inflammation, granulation, and tissue remodeling)3,4 that can affect how spectral imaging methods interpret both structural and functional parameters in tissue. With a thermal insult, there can be disruption of the vascular network, leaving blood trapped within the affected tissue. As trapped hemoglobin breaks down, the byproducts (e.g., methemoglobin) could then contribute to the measured spectra.5 This process may have previously uncharacterized consequences for optical imaging methods as it may interfere with standard methods for interpreting and quantifying absorption data in terms of parameters such as tissue oxygen saturation.

While multispectral approaches have been applied toward the early detection and triage of burn wounds and shown great potential, these instruments and approaches often use limited spectral sampling and resolution.1,2,6 Spatial frequency domain imaging (SFDI) has been of particular interest in this application as it quantifies absorption and scattering optical properties of \(\text{in-vivo}\) tissue at every wavelength independently using the diffuse reflectance response from tissue as a function of the pattern frequency projected and a scaled Monte Carlo to model photon migration.8 This enables separation of changes in tissue structure from those resulting from changes in absorption characteristics without any additional presumed scattering model or chromophores.2,9,10 When it comes to determining tissue constituents, many other analysis techniques depend on \(a\ priori\) models that presume all potential sources of optical contrast within tissue in order to interpret measured data. Though blood breakdown products such as methemoglobin are not usually considered in optical device measurements of tissue oxygen saturation, it has already been suggested that they might play a significant role in burn wounds.11,12

Our primary objective is to investigate whether spectral signatures from methemoglobin (\(\text{MetHb}\)) are present, \(\text{in vivo}\), in optical measurements of burn wounds and what influence they may exert in the accurate and reliable determination of other tissue functional parameters. Additionally, we will evaluate how these blood breakdown products might impact the performance of a commercial multispectral imager that has coarse spectral resolution and relatively few illumination wavelengths. This is done as a side-by-side comparison with the high spectral resolution approach using the same set of \(\text{in vivo}\) burn data as described as follows.

In this investigation, spectrally resolved tissue optical properties were calculated using a technique called spatial frequency domain spectroscopy (SFDS).10,11 Here, the reflectance data were measured by a custom-built, handheld spectral imaging system, described in greater detail elsewhere.12 This device projects broadband (450 to 1000 nm) illumination of sinusoidal intensity and then detects the spatial frequency-dependent responses from tissue along a ~3-cm line, at ~1 nm spectral resolution. In this study, five evenly spaced spectral frequencies were employed ranging from 0 to 0.2 mm~1. Three phases (i.e., 0 deg, 120 deg, and 240 deg) of each frequency were projected, as has been our convention, so that the frequency-dependent reflectance can be extracted at each spatial location independent from adjacent measurement locations.10

We have applied this handheld SFDS system in an established porcine burn wound model of graded burn severity.11 In this study, a specialized tool was used to create a series of graded burns on the back of a Yorkshire pig, 3 cm in diameter. The SFDS spectral imager measured the multiply scattered

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light from both burn region and adjacent tissue with ~3 nm spectral resolution over several distinct longitudinal time points that allow us to compare preburn, acutely postburn, and at a couple of time points that correspond with those that are indicated as important time points for burn severity assessment (out to 3 days postburn). All experiments followed protocols reviewed and approved by the UC Irvine Institutional Animal Care and Use Committee (IACUC #2015-3154).

Tissue absorption coefficient spectra are then extracted from these measurements and subsequently decomposed to identify all physiologic sources of absorption contrast present in the in vivo tissues, including those of hemoglobin breakdown products, over the wavelength range of 450 to 1000 nm. From the spectral components identified by SFDS, we can demonstrate how the presence and dynamics of the methemoglobin in the wound healing process will impact the concentration estimation of other functional tissue parameters if not properly accounted for.

Using a validated spectral bandwidth emulation approach, we can transform SFDS data to mimic the same spectral qualities of multispectral imagers within the visible and near-infrared ranges. In this investigation, we consider the spectral performance of a commercially available, LED-based SFDI device: the OxImager RS, (Modulated Imaging, Inc.). Here, chromophore concentrations calculated from the emulated spectral data from the commercial instrument will be compared to those determined using the full spectral resolution of SFDS. This particular instrument was selected in this evaluation as it is has been used in several investigations of burn wounds and remains actively engaged in our ongoing studies. The spectral characteristics of this LED-based imager used for this evaluation have been published elsewhere.

Figure 1 shows the evolution of tissue absorption within the burned tissue over time. Here, the spectra are derived from the average of a ~1-cm line (~300 pixels) within the center of the 3-cm wide burn. Spectra recorded at earlier time points are included in visualization of later time points to help illustrate the shifts that occur in relative magnitude and shape of the absorption spectra. In the case of the 10-s burn (superficial), the spectral changes are slight, indicative of minimal tissue damage and wound healing response. There was a greater change in the 20-s burn (superficial partial thickness); however, the spectrum returned to its preburn shape and magnitude by 72 h, potentially indicating a complete recovery. Both 30 and 40 s burns (deep partial and full thickness) not only fail to return to baseline by 72 h, an additional, broad absorption feature becomes readily apparent by 24 h. This feature is not replicated or explained by combinations of common tissue chromophores (i.e., oxy- and deoxyhemoglobin, water, melanin, lipids, etc.). Given the shape and location of absorption bands, this burn-induced spectral feature correlates strongly with hemoglobin breakdown products, e.g., MetHb. To this end, we used the absorption spectrum for pure MetHb from Zijlstra et al.

Without the inclusion of MetHb in the spectral analysis, errors in the determination of several other tissue parameters will arise, as shown in Fig. 2. This figure depicts the spectral fits to the measured absorption spectra from the 30-s burn case (deep partial thickness burn). Here, the results of two least-squares fits are shown. The first fit result presumes oxy- and deoxyhemoglobin, water, and melanin are the only absorbing constituents present in the tissue volume; the second fit result also includes MetHb in this spectral model. Using the normalized root mean square error as the cost function for a goodness of fit metric, including MetHb maintains a goodness of fit to within 85% of the measured data over all time points, but without its inclusion, the agreement can degrade to ~56%.

Inclusion of MetHb in the spectral fitting will not only improve the goodness of fit but also have significant impact on the quantification of other tissue chromophores and physiological parameters. Within the context of the four burn severities...
investigated here, tissue oxygen saturation, StO₂, is underesti-
mated by as much as 20% within the first 3 days postburn
and the tissue water fraction, is underestimated by as much
as 78% when MetHb is not included in the fitting the measured
SFDS absorption spectra. Largely, the magnitude of these
underestimation errors directly correlate with increased concen-
tration of MetHb within tissue volumes, hence these estimation
erors increase with burn severity (i.e., 30 and 40 s burns), and
with time (i.e., 24 and 72 h time points). It is worth noting that
even in less severe burns, such as the case of the superficial
partial thickness (20 s) burns, StO₂ and water fraction may
be underestimated by 12% and 8%, respectively, 24 h after
the injury.

Lastly, we have also determined that even with only eight
spectral bands that span both visible and near-infrared wave-
length regimes, a multispectral SFDI imager can account for
MetHb, producing functional tissue parameters that agree
with the high spectral resolution data (SFDS). Through emulat-
ing the OxImager’s spectral profile with all the collected SFDS
data, we can directly evaluate the impact that a reduced set of
spectral bands and resolution may have on the calculation of
tissue optical properties. In this case, this particular multi-
spectral imager would determine StO₂ within 3.9% and water
fraction within 6.9% of the values calculated using all spectral
content collected by SFDS. These results include all burn types
and time points considered in this initial investigation.

While the goodness of fit metric, shown in Fig. 2, demon-
strates that incorporating a pure MetHb spectrum in our fitting
model significantly reduces residual features between measure-
ment and model and supports the assertions of others, it may
suggest that quantification of MetHb may provide addi-
tional and complementary information to assess and character-
ize burn wound severity. While parameters such as StO₂ and
water fraction (edema) may indicate the tissues functional
response to the injury, MetHb may indicate a measure of the
amount of damage. The combination of these parameters may
present unique opportunities to advance burn wound assessment
toward personalized medicine where it is critical to know not
just how much damage has occurred within the wound, but
whether the patient has initiated a wound healing response and
whether that response will be sufficient to heal the wound on
its own.

In conclusion, we have demonstrated that additional hemo-
globin species will arise in tissue from burn wound injuries and
dynamically vary in concentration during the wound healing
process. Based on the spectral characterization from in vivo
burn wound measurements, these absorption features correlate
to hemoglobin breakdown products, e.g., MetHb. Additionally,
we have also demonstrated that it is important to include MetHb
in any multispectral image analysis in order to produce robust

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**Fig. 2** Measured and fitted tissue absorption spectra for the 30 s (deep partial thickness) burn over time. Solid lines represent the measured absorption spectra. Dashed lines represent the linear least-squares fit produced when only HbO₂, Hb, water, and melanin are used as a spectral basis set. Dotted lines represent the fit when pure MetHb is added to the basis set.

**Fig. 3** Methemoglobin concentration over time. Inset figure shows the positive correlation of the calculated concentration to burn severity (time duration of burn injury) after 24 h.
estimates of other tissue parameters, such as StO2 and water fraction.

Disclosures
Dr. Durkin has a financial interest in Modulated Imaging, Inc., which developed the Reflect RS™. However, Dr. Durkin does not participate in the management of Modulated Imaging and has not shared these results with that company. Conflicts of interest have been disclosed and carefully managed in accordance with the University of California and NIH policies. The other authors have no financial interests or commercial associations that might pose or create a conflict of interest with the information presented in this article.

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